

# Multi-subject Diffusion MRI Tractography via a Hough Transform Global Approach

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**Introduction:** Multi-subject tractography in Diffusion-Weighted MRI is a valuable technique for statistical analysis of the brain’s anatomical connectivity and population studies (e.g., Leemans *et al.* 2006; Voineskos *et al.* 2008; Jbabdi *et al.* 2009). Prior approaches are based on the post processing of tractography results from individual subjects, and generally require aligning the tracts and mapping them into a common fiber coordinate system. In this work, we introduce a simultaneous multi-subject tractography technique using high angular resolution diffusion imaging (HARDI). It takes as input a single representative volume, where the HARDI data from all the subjects are non-linearly integrated, and generates population-representative tracts. The tractography algorithm is run only once, and no tract alignment is necessary.

**Methods:** We extend the *Hough transform*-based global approach introduced in (Aganj *et al.* 2009) to multi-subject tractography. The algorithm uses a voting process on all possible three-dimensional curves in the volume, assigns a score to each of them, and chooses those with the highest scores as potential tracts. For a single subject, the score given to each curve is defined as  $\int \left( \log \left[ ODF \left( \vec{x}(s), \vec{t}(s) \right) GFA \left( \vec{x}(s) \right) \right] + \lambda \right) ds$ , where  $\vec{x}(s)$  and  $\vec{t}(s)$  are respectively the location and the unit tangent vector of the curve under consideration at the arc length  $s$ ,  $ODF$  is the orientation distribution function,  $GFA$  is the generalized fractional anisotropy, and  $\lambda$  is a positive constant. The linearity of the score with respect to the logarithms of  $ODF$  and  $GFA$  makes the extension of this method to multiple subjects both unique and straightforward. We perform this by first registering the HARDI volumes, following e.g. (Chiang *et al.* 2008), and then running the algorithm on a single volume composed of the voxel-wise sum of the integrands for all the subjects. Since the sum of the logarithms of the  $ODFs$  equals the logarithm of their product, we reconstruct for each voxel an effective  $ODF$  in spherical harmonic basis by computing the product of the  $ODFs$  across the subjects. We eventually use it in the algorithm, thereby obtaining for multiple subjects the same tractography algorithm as for a single subject, only with a new “equivalent  $ODF$ .”

**Results:** HARDI data was obtained from four subjects, with each dataset containing 27 diffusion-weighted images acquired at  $b=1100$  s/mm<sup>2</sup>. Imaging matrix was  $128 \times 128 \times 21$  with voxel size  $1.8 \times 1.8 \times 5$  mm<sup>3</sup>. The  $ODFs$  were computed in spherical harmonic basis, sharpened, and then registered to a common space (Chiang *et al.* 2008). The tractography algorithm was first tested on each of the four individual volumes, and then on the single equivalent volume. As the figures demonstrate, by combining the volumes noticeable improvement in the results is observed. In particular, the fibers are less scattered and better concentrated in major fiber bundles. Note how corticospinal tracts and the splenium of corpus callosum are enhanced.

**Conclusions:** We have introduced a global approach for multi-subject tractography, based on the voting process provided by the *Hough transform*. We presented experimental results on four human brain

HARDI datasets, and showed that using this approach, data from multiple subjects can be non-linearly combined and exploited to obtain population statistics and more accurate tractography results.

### References:

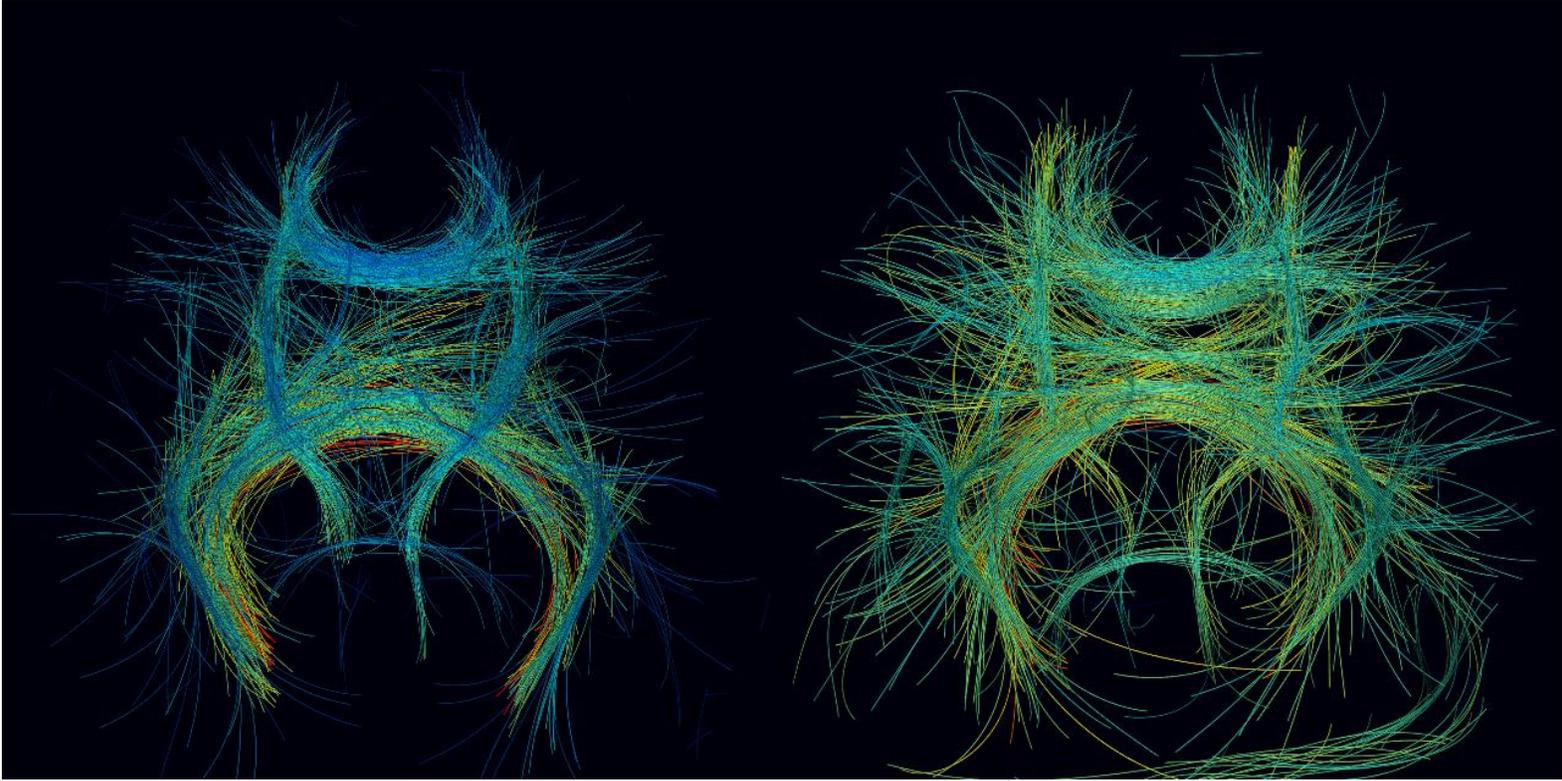
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(four subjects combined)

(one of the subjects)

A tilted coronal/axial view of the tractography results.